





Adaptive Radiotherapy in patient Radiation Protection

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Line

- Adaptive RT
- What about its utility?
- Patient's radioprotection during radiotherapy
- Doses during adaptive radiotherapy using ionizing radiations: are these clinically relevant?
- RM adaptive radiotherapy (not only for radioprotection reasons)
- Problems in ART: dose accumulation and deformable image registration
- Conclusions

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Adaptive radiotherapy

- Radiotherapy has evolved significantly over the years. Traditionally, treatment plans were based on
 initial scans used throughout the treatment course, accounting for changes in the patient's anatomy
 by additional margins to targets.
- However, the field has moved towards decreasing margins with the advancement of delivery and targeting accuracy in order to decrease toxicity, and the increasing use of image guidance has illuminated patient anatomical changes such as organ deformation, weight loss, tumour shrinkage, and even biological changes that are unaccounted for by the conventional approach.

Adaptive radiotherapy (ART) addresses this by adjusting treatment plans according to these changes.

ART can be conducted in two ways:

- online (adjustments made during treatment sessions)

- offline (adjustments made between treatment sessions).

Nevertheless, as demonstrated in panels A3-4 and B3-4, when there is a **disparity between the anatomy on the treatment day and the anatomy during the simulation, as the treatment plan becomes increasingly sophisticated and tightly conformal to the original targets, the anatomical changes can lead to a greater deviation from the initial intention**.

Consequently, the coverage of the tumour dose is compromised, and the OARs receive a higher dose than planning



Dona Lemus, O.M.; Cao, M.; Cai, B.; Cummings, M.; Zheng, D. Adaptive Radiotherapy: Next- Generation Radiotherapy. *Cancers* **2024**,*16*,1206. https://doi.org/ 10.3390/cancers16061206



- ART signifies a fundamental change from conventional radiotherapy, as it involves dynamically reoptimizing the treatment plan to accommodate changes in the patient's anatomy.
- This guarantees the preservation of accurate radiation dosage to the tumour while specifically protecting nearby OARs, thus optimizing the therapeutic ratio that can be achieved with advanced radiotherapy technology.

Table 1. Summary of offline vs. online ART.

| | Offline ART | Online ART |
|-----------|---|---|
| Frequency | Offline ART involves evaluation/adjustments to the treatment plan in between treatment sessions, with the patient off the table. Plan adjustments are based on anatomy imaged at a certain timepoint and applied for later sessions. It is often applied in lower frequency such as mid-treatment, biweekly, or weekly. | Online ART involves evaluations/adjustments based on the session anatomy, while the patient stays on the treatment table, and is applied for th treatment of the same session. It is currently mor often applied in each treatment session. |

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| Complexity | When performed less frequently, it is generally less resource-intensive compared to online ART. At the same time, it could still be staff-time-demanding if offline ART has a less streamlined or automated workflow than available in online ART. | Online ART can be more complex and resource-intensive compared to offline ART because it requires specialized equipment and software and may be carried out more frequently. | |

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| Treatment planning | Offline ART is not conducted on patient images obtained in the session the adaptive plan is intended to be applied. Instead, planning is conducted offline on previously obtained images to apply in future sessions. | It allows for a highly individualized and precise treatment plan for each session, taking into account the new anatomy in each treatment session. The adaptive plan is made based on the session image and applied to the same session. |

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| Treatment planning | Offline ART is not conducted on patient images obtained in the session the adaptive plan is intended to be applied. Instead, planning is conducted offline on previously obtained images to apply in future sessions. | It allows for a highly individualized and precise treatment plan for each session, taking into account the new anatomy in each treatment session. The adaptive plan is made based on the session image and applied to the same session. | | | |
| Clinical Applications | It is suitable for patients with tumors, OARs, and body habitus that are less likely to experience rapid anatomical changes and when the tumor is relatively distant from critical structures. It is commonly employed in situations such as head and neck cancers. Patient setup changes could also trigger the need for offline adaptation. | Used for cases where anatomical changes are expected on a daily basis. It is commonly employed in situations such as abdominal and pelvic malignancies. Based on the optimal trade-off between clinical benefits and required resources, the online ART platform may also be used for various disease sites to apply daily, weekly or on-demand plan adaptation | | | |

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Basic workflow ART



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Basic principles of radioprotection

- Justification of the exposition
- Optimization of the dose
- Limitation of the maximal dose

Basic principles of radioprotection for patients treated with RT

- Justification of the exposition \rightarrow radical/palliative treatment of the tumor \rightarrow informed consent
- Optimization of the dose → great attention to OAR, to dose distribution to G and CTV, to reduce unnecessary dose out of the target
- Limitation of the maximal dose → the maximal doses for general population are too low for patients treated with RT → but also for these patients the attention has to be posed to reduce the unnecessary dose and to deliver the minimum necessary dose

Adaptive Radiation Therapy

Radiation exposure during the acquisition of the CBCT scan, while minimal compared with the dose delivered during RT treatment, nevertheless prevents the use of CBCT for repeated images throughout the fraction; therefore, CBCT cannot be used for real-time ART or intrafraction motion assessment (46,56). The imaging dose for kilovoltage-CBCT typically ranges from 0.2 to 2 cGy per image (20,29). Skin dose has been measured to be a fraction of a centigray for low-dose head and neck imaging and 7 cGy for high-dose pelvic imaging (56).

In summary, the key advantages of CBCT-based ART include its ease of integration into the RT workflow and potential for rapid imaging and replanning, leading to feasible time frames for online adaptation. The major drawback is the inferior image quality due to poor resolution, scatter, and artifacts, which leads to reduced soft-tissue contrast and increased dosimetric uncertainty. As online ART relies heavily on the quality of onboard imaging for treatment adaptation, there has been much enthusiasm about MRI platforms for online ART. Hybrid systems that combine linear accelerators with onboard MRI (MRI-linear accelerator systems) are commercially available and have been used in most clinical implementations of online ART to date (46), including in patients with lung tumors (38), liver and other abdominal malignancies (22), pancreas cancer (28), colorectal cancer (23), prostate cancer (21,37), and adrenal metastases (36).

While implementing MRI-guided ART can require a substantial investment of resources and pose many technical challenges, the increased soft-tissue resolution over CBCT and the potential for real-time and functional imaging offer important advantages to MRI-linear accelerator implementation for ART

Dose assessment for daily cone-beam CT in lung radiotherapy patients and its combination with treatment planning

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Abstract

With the increased use of X-ray imaging for patient alignment in external beam radiation therapy, particularly with cone-beam computed tomography (CBCT), the additional dose received by patients has become of greater consideration. In this study, we analysed the radiation dose from CBCT for clinical lung radiotherapy and assessed its relative contribution when combined with radiation treatment planning for a variety of lung radiotherapy techniques. The Monte Carlo simulation program ImpactMC was used to calculate the 3D dose delivered by a Varian TrueBeam linear accelerator to patients undergoing thorax CBCT imaging. The concomitant dose was calculated by simulating the daily CBCT irradiation of ten lung cancer patients. Each case was planned with a total dose of 50-60 Gy to the target lesion in 25-30 fractions using the 3DCRT or IMRT plan and retrospectively planned using VMAT. For each clinical case, the calculated CBCT dose was summed with the planned dose, and the dose to lungs, heart, and spinal cord were analysed according to conventional dose conformity metrics. Our results indicate greater variations in dose to the heart, lungs, and spinal cord based on planning technique, (3DCRT, IMRT, VMAT) than from the inclusion of daily cone-beam imaging doses over 25-30 fractions. The average doses from CBCT imaging per fraction to the lungs, heart and spinal cord were 0.52 \pm 0.10, 0.49 \pm 0.15 and 0.39 \pm 0.08 cGy, respectively. Lung dose variations were related to the patient's size and body composition. Over a treatment course, this may result in an additional mean absorbed dose of 0.15-0.2 Gy. For lung V5, the imaging dose resulted in an average increase of ~ 0.6% of the total volume receiving 5 Gy. The increase in V20 was more dependent on the planning technique, with 3DCRT increasing by 0.11 \pm 0.09% with imaging and IMRT and VMAT increasing by 0.17 \pm 0.05% and 0.2 \pm 0.06%, respectively. In this study, we assessed the concomitant dose for daily CBCT lung cancer patients undergoing to the normal lungs from daily CBCT was found to range radiotherapy. nen the patient was treated with 25-30 fractions. Consideration of potential variation in relative biological effectiveness between kilovoltage imaging and megavoltage treatment dose was outside the scope of this study. Regardless of this, our results show that the assessment of imaging dose can be incorporated into the treatment planning process and the relative effect on overall dose distribution was small compared to the difference among planning techniques.

Keywords: 3DCRT; CBCT Dose; Daily CBCT; IMRT; Lung cancer; Monte Carlo; VMAT.

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nvestigation of the radiation dose from cone-beam CT for image-guided radiotherapy: A comparison of methodologies

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Fig. 4. Comparison of TG111, CBDI, IAEA, and CTDI methodologies on the OBI and XI imaging systems for pelvis (a) and thorax (b) protocols. The IAEA was not evaluated for OBI thorax. Comparison of CBDI, IAEA, and CTDI methodologies for OBI standard head and XI head protocols is shown in (c). Error bars represent one standard deviation from repeated measurements.

Clinical dosimetric confirmation of adaptive procedures

Abstract

Background Daily adaptive radiation therapy (ART) of patients with non-small cell lung cancer (NSCLC) lowers organs at risk exposure while maintaining the planning target volume (PTV) coverage. Thus, ART allows an isotoxic approach with increased doses to the PTV that could improve local tumor control. Herein we evaluate daily online ART strategies regarding their impact on relevant dose-volume metrics. **Methods** Daily cone-beam CTs $(1 \times n = 28, 1 \times n = 29, 11 \times n = 30)$ of 13 stage III NSCLC patients were converted into synthetic CTs (sCTs). Treatment plans (TPs) were created retrospectively on the first-fraction sCTs (sCT₁) and subsequently transferred unaltered to the sCTs of the remaining fractions of each patient (sCT_{2-n}) (IGRT scenario). Two additional TPs were generated on sCT_{2-n} : one minimizing the lung-dose while preserving the D_{95%}(PTV) (isoeffective scenario), the other escalating the $D_{95\%}$ (PTV) with a constant V_{20Gy} (lung_{ipsilateral}) (isotoxic scenario). **Results** Compared to the original TPs predicted dose, the median D_{95%}(PTV) in the IGRT scenario decreased by 1.6 Gy \pm 4.2 Gy while the V_{20Gy}(lung_{ipsilateral}) increased in median by 1.1% \pm 4.4%. The isoeffective scenario preserved the PTV coverage and reduced the median V_{20Gy} (lung_{ipsilateral}) by 3.1% ± 3.6%. Furthermore, the median $V_{5\%}$ (heart) decreased by 2.9% \pm 6.4%. With an isotoxic prescription, a median dose-escalation to the gross target volume of 10.0 Gy \pm 8.1 Gy without increasing the V_{20Gy}(lung_{ipsilateral}) and V_{5%}(heart) was feasible. **Conclusions** We demonstrated that even without reducing safety margins, ART can reduce lung-doses, while still reaching adequate target coverage or escalate target doses without increasing ipsilateral lung exposure. Clinical benefits by means of toxicity and local control of both strategies should be evaluated in prospective clinical trials. **Keywords** Adaptive radiation therapy, stage III NSCLC, Isotoxic dose-escalation, Isoeffective organ at risk sparing

lung

prostate

Inter-fraction organ variations cause deviations between planned and delivered doses in patients receiving radiotherapy for prostate cancer. This study compared planned (D_P) vs accumulated doses (D_A) obtained from daily cone-beam computed tomography (CBCT) scans in high-risk- prostate cancer with pelvic lymph nodes irradiation. An intensity-based deformable image registration algorithm used to estimate contours for D_A was validated using geometrical agreement between radiation oncologist's and deformable image registration algorithm propagated contours. Spearman rank correlations (r_s) between geometric measures and changes in organ volumes were evaluated for 20 cases. Dose-volume (DV) differences between D_A and D_P were compared (Wilcoxon rank test, p < 0.05). A novel region-of-interest (ROI) method was developed and mean doses were analyzed. Geometrical measures for the prostate and organ-at-risk contours were within clinically acceptable criteria. Inter-group mean (\pm SD) CBCT volumes for the rectum were larger compared to planning CT (pCT) (51.1 \pm 11.3 cm³ vs 46.6 \pm 16.1 cm³), and were moderately correlated with variations in pCT volumes, rs = 0.663, p < 0.01. Mean rectum DV for D_A was higher at V30-40 Gy and lower at V70-75 Gy, p < 0.05. Mean bladder CBCT volumes were smaller compared to pCT (198.8 \pm 55 cm³ vs 211.5 \pm 89.1 cm³), and was moderately correlated with pCT volumes, rs = 0.789, p < 0.01. Bladder D_A was higher at V30-65 Gy and lower at V70-75 Gy (p < 0.05). For the ROI method, rectum and bladder D_A were lower at 5 to 10 mm (p < 0.01) as compared to D_P , whilst bladder D_A was higher than D_P at 20 to 50 mm (p < 0.01). Generated D_A demonstrated significant differences in organ-at-risk doses as compared to D_P. A well-constructed workflow incorporating a ROI DV-extraction method has been validated in terms of efficiency and accuracy designed for seamless integration in the clinic to guide future plan adaptation.

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Size-specific Effective Dose (SED)

- Results from the Monte Carlo simulations carried out in this study have compared values for SEDs between phantoms of different stature.
- This shows that patients who are shorter or lighter will receive (significantly) higher doses if similar exposure factors and field sizes are used for CBCT scans on all patients.

"A person who is 5 cm shorter will receive a SED that is 3%–7% greater for a chest scan and 4%–10% greater for a pelvis scan.

A person who is 10 kg lighter will receive a dose that is 11%–14% greater for a chest scan and 10%–13% greater for a pelvis scan.

The differences amount to 0.7 mSv to 1.6 mSv from one scan, but since radiotherapy treatments are often given in 20–30 fractions, the increase in cumulative dose can be significant if protocols are not optimised"

Size-specific Effective Dose (SED)

The culture of adapting imaging exposure parameters and field sizes to individual patients is less well established in IGRT than in diagnostic radiology





Figure 2. Bar charts showing the percentage of radiotherapy centres in different countries that adjust the field size for kV IGRT planar and kV CBCT imaging in a recent survey of imaging practices [10].

Adaptive Radiation Therapy: A Review of CT-based Techniques

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| Clinical Site | ART Type | No. of Patients | Clinical Implementa- tion of ART? | Fractionation Scheme | OAR | OAR Dose Sparing |
|-------------------------------------|------------------------|--------------------|--------------------------------------|---|---|---|
| Oropharyngeal (14) | Offline | 22 | Yes | 66–72 Gy, 30–33 fractions | Contralateral parotid | 0.6 Gy or 2.8% |
| | | | | | Ipsilateral parotid | 1.3 Gy or 3.9% |
| Head and neck (13) | Offline | 13 | No | 70 Gy, 35 fractions | Parotids | 3.1 Gy |
| Cervix (10) | Offline | 9 | Yes | 45 Gy, 25 fractions | Rectum V95% | 3.20% |
| | | | | | Bladder V95% | 1.10% |
| Pancreas (35) | Online MRI-guided | 36 | No | 40 Gy, 5 fractions | Duodenum V33 Gy | 0.3 cm ³ |
| Abdominopelvic (23) | Online MRI-guided | 5 | Yes | | Small bowel V50 Gy (one patient) | 67.8 cm ³ |
| Adrenal (36) | Online MRI-guided | 52 | Some patients | 24–60 Gy, 3–8 fractions | Stomach NTCP | 8.70% |
| Bladder (26) | Online CBCT- guided | 3 | Yes | | Bowel cavity V45 Gy | 24%-30% |
| Prostate (15) | Online CBCT- guided | 25 | No | 54 Gy, 27 fractions + prostate boost | Bladder D90% Rectum D90% | 13.10% 6.50% |
| Abdominal oligo- metastatic (40) | Online CBCT- guided | 8 | No | 50 Gy, 5 fractions | Stomach V36 Gy Duodenum V36 Gy Small bowel V36 Gy Large bowel V36 Gy | 0.36 cm ³ 0.96 cm ³ 1.09 cm ³ 0.8 cm ³ |

Organ at Risk-sparing Achieved by Adaptive Radiation Therapy

Note.—ART = adaptive radiation therapy, CBCT = cone-beam CT, D90% = minimum dose that 90% of the structure is receiving, NTCP = normal tissue complication probability, OAR = organ at risk, V33 Gy = volume receiving more than or equal to 33 Gy, V36 Gy = volume receiving more than or equal to 36 Gy, V45 Gy = volume receiving more than or equal to 45 Gy, V50 Gy = volume receiving more than or equal to 50 Gy, V95% = volume receiving at least 95% of the prescription dose.

| : Coverage | of Clinical Tar | gets by A | daptive Radiation | Therapy | | | | | Clinica | l Outcomes | of Adaptiv | ve Radiation Ther | apy | | | |
|-------------------------------------|-----------------------|-----------|-----------------------------|-------------------------------|-------------------|------------|-----------------|-------------------------------|--|---|---|---|---|--|--|------------------------------|
| | | | | | Target | Coverage | Clinical T | arget Volume | | | No. of | Fractionation | Clinical O | Outcome | Toxicity | |
| Clinical Site | APT Tupe | No. of | Clinical Implementation? | Fractionation | Metric | Change in | Metric | Change in Volume | Clinical Site | ART Type | Patients | Scheme | Metric Evaluated | Outcome | Metric Evaluated | Outcome |
| Oropharyngeal (14) | Offline | 22 | Yes | 66–72 Gy, 30–33 frac- | Evaluated | Coverage | CTV volume | -5% | Oropharyngeal (14) | Offline | 22 | 66–72 Gy, 30–33 frac- tions | Local control Regional control | 100% 95% | Comparison to IMRT | Comparable |
| Head and neck (13) | Offline | 13 | No | 70 Gy, 35 frac- tions | CTV 70 D98% | +0.6% | PTV vol- ume | No sig- nificant change | NSCLC (30) | Offline | 50 | 45–75 Gy | Local control Median PFS Median OS | 70% 8.3 months 30.5 months | Comparison to RTOG 9410 clinical trial | Reduced |
| NSCLC (30) | Offline | 50 | Yes | 45–75 Gy | OTT | | CTV volume | -42% | Adrenal (36) | Online MRI- | 52 | 24–60 Gy, 3–8 fractions | | | ≥ grade 3 toxicity | 0% |
| Cervix (10) | Offline | 9 | Yes | 45 Gy, 25 frac- tions | CTV cov- erage | Equivalent | t PTV V95% | -87 cm ³ | Prostate (37) | guided | 101 | 36.25 Cur 5 frag | | | > grade 2 early CI | 22.80% |
| Pancreas (35) | Online MRI- guided | 36 | No | 40 Gy, 5 frac- tions | GTV V95% | +1.1 Gy | | | 110state (37) | MRI- | 101 | tions | - | | toxicity | 504 |
| Abdominopelvic (23) | Online MRI- guided | 5 | Yes | | PTV V95% | +14% | | | | guided | | | | | 2 grade 2 early GO toxicity | J%0 |
| Abdomen (22) | Online MRI- guided | 20 | Yes | 50 Gy, 5 frac- tions | GTV V100% | +4% | | | | | | | | | Comparison to HYPRO study | Reduced |
| | 5 | | | | PTV V95% | +3.2% | | | Lung (38) | Online MRI- | 50 | | 12 months, local control | 95.60% | ≥ grade 2 toxicity | 30% |
| Lung (38) | Online MRI- guided | 50 | Yes | | PTV V100% | +4.4% | | | | guided | | | 12 months, OS 12 months, DFS | 88% 64% | \geq grade 3 toxicity | 8% |
| Bladder (26) | Online CBCT guided | - 3 | Yes | | PTV V95% | +11.4% | PTV vol- | -42% | Abdomen (22) | Online | 20 | 50 Gy, 5 frac- | 6 months, PFS | 89.10% | ≥ grade 3 acute toxicity | 0% |
| Prostate (15) | Online CBCT guided | - 25 | No | 54 Gy, 27 fractions + | CTV D98% | +2.9% | unic | | | MRI- guided | | tions | 12 months, OS | 75% | | |
| Cervix (11) | Online CBCT guided | - 13 | No | 45 Gy, 25 frac- tions + LN | CTV V95% | +7.9% | | | Note.—ART = a ated versus conve small cell lung ca | daptive radiat ntionally frac ncer, OS = ov | tion therapy, ctionated R1 verall surviva | , DFS = disease-free I for patients with lo al, PFS = progression | survival, GI = gasti ocalized prostate can n-free survival, RTC | ointestinal, GU ncer, IMRT = ir DG = Radiation | J = genitourinary, HYPRO ntensity-modulated RT, NS Therapy Oncology Group. | = hypofraction CLC = non– |
| Rectum (11) | | 15 | | 50 Gy, 25 frac- tions | CTV V95% | +1.5% | | | | | | | | | | |
| Prostate (25) | Online CBCT guided | - 18 | Yes | 36.6 Gy, 6 frac- tions | PTV D99% | +6.7% | | | | | | | | | | |
| Rectum (24) | Online CBCT guided | - 12 | Yes | 25 Gy, 5 frac- tions | PTV V95% | Improved | | | | | | | | | | |
| Abdominal oligo- metastatic (40) | Online CBCT guided | - 8 | No | 50 Gy, 5 frac- tions | PTVopt V95% | +10.15% | | | | | | | | | | |

Note.—ART = adaptive radiation therapy, CBCT = cone-beam CT, CTV = clinical target volume, D98% = minimum dose that 98% of the target is receiving, GTV = gross tumor volume, LN = lymph node, NSCLC = non–small cell lung cancer, PTV = planning target volume, PTVopt = PTV optimization structure, V95% = volume receiving at least 95% of the prescription dose, V100% = volume receiving at least 100% of the prescription dose.

To conclude (1):

A few dosimetric evaluations are available in the literature regarding the contribution of CT scanning for ART to the dose received by the patient.

These doses are in general negligible when compared with the advantages of ART in terms of OAR sparing, better PTV coverage and reduction of the PTV volume.

The dose received because of ART by the patient varies with the target of the treatment and the PTV volume. Lighter and shorter people may receive higher doses by cone beam scanning and specific protocols may help to further reduce the dose received for them.

Is there a future?

Probably the MR-ART can be the future







| Table 4: Comparison between MRI | -based and CBCT-based Online Adaptive R | adiation Therapy Approaches |
|---|---|--|
| Feature | MR-linac Online ART | CBCT-based Online ART |
| Image quality | Superior (46) | Inferior image quality and soft-tissue definition (6,20,33,46,47) |
| Image artifacts | Susceptibility, motion, distortion (6) | Hardening, motion, scatter, ring, aliasing, mis- alignment (20,33,49) |
| Inaccuracies in determining size of target | NA | Cervix, prostate (57,58) |
| Information about physiologic char- acteristics of tissue (eg, diffusion, perfusion) | Superior | NA |
| Functional or quantitative imaging | Possible; not yet ready for clinical implementa- tion (6,16) | NA |
| Limited field of view | Limited to 50 cm (6) | Limited to 16 cm in the longitudinal direction (6,55) |
| Image acquisition time | Longer (limited sequences within 2 min) (46) | Shorter (within 1–2 min) (46) |
| Conversion of image-of-the-day to electron density map | Synthetic CT; bulk density assignment to ana- tomic structures; multimodality DIR (6,16) | Conversion to Hounsfield units via DIR, CBCT calibration curves, dose deformation* (33,52) |
| Imaging-related radiation exposure | None | Up to 10 cGy per scan; typically, 0.2 cGy–2 cGy (6,20,29,46,56) |
| Continuous imaging (eg, motion gating, real-time tracking of dose accumulation) | Possible (6) | Limited by radiation exposure |
| Specialized training for MRI-based RT planning | Required (46) | NA |
| Radiation and MRI-compatible facili- ties | Required (46) | NA |
| Cost of linear accelerator, structural investment | Very high (46) | Reduced compared with MRI (46) |
| Limits on patient size | More restrictive (46) | Less restrictive (46) |
| C <mark>ontraindications</mark> (claustrophobia, metallic implants) | Yes (46) | No (46) |
| PP1 1 . | T (==== 1.0) | |



| Table 4: Comparison between MRI | -based and CBCT-base | d Online Adaptive R | adiation Therapy Approaches | | | | |
|--|---|---|--|--|--|--|--|
| Feature | MR-linac Online ART | | CBCT-based Online ART | | | | |
| Image quality | Superior (46) | | Inferior image quality and soft-tissue definition (6,20,33,46,47) | | | | |
| Image artifacts | Susceptibility, motion, d | listortion (6) | Hardening, motion, scatter, ring, aliasing, mis- alignment (20,33,49) | | | | |
| Inaccuracies in determining size of target | NA | | Cervix, prostate (57,58) | | | | |
| Information about physiologic char- acteristics of tissue (eg, diffusion, perfusion) | Superior | | NA | | | | |
| Functional or quantitative imaging | Possible; not yet ready fo tion (6,16) | or clinical implementa- | NA | | | | |
| Limited field of view | Limited to 50 cm (6) | | Limited to 16 cm in the longitudinal direction (6,55) | | | | |
| Image acquisition time | Longer (limited sequenc | es within 2 min) (46) | Shorter (within 1-2 min) (46) | | | | |
| Conversion of image-of-the-day to electron density map | Synthetic CT; bulk dens tomic structures; mult | ity assignment to ana- timodality DIR (6,16) | Conversion to Hounsfield units via DIR, CBCT calibration curves, dose deformation* (33,52) | | | | |
| Treatment duration | Longer (21,22,46) | | Potentially shorter (11,26,27) | | | | |
| Electron return effect [†] | Significant [‡] | | NA | | | | |
| Significant geometric distortion | Due to magnetic-field gr field inhomogeneities | radient nonlinearities, § | NA | | | | |
| Patient-dependent geometric distor- tions | Possibly significant | | NA | | | | |

Note.—ART = adaptive radiation therapy, CBCT = cone-beam CT, DIR = deformable image registration, MR-linac = MRI-linear accelerator, NA = not applicable.

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- * Poorer image quality of CBCT images can lead to dose calculation inaccuracies.
- [†] The electron return effect refers to electron path distortion and increase in radiation dose delivery near air-tissue interfaces. [‡] The electron return effect with MRI can be addressed with Monte Carlo algorithms and multiple fields.

- [§] MRI geometric distortion can be accounted for by image processing algorithms.
- Patient-dependent geometric distortions result from local magnetic field inhomogeneities.







reference

#1



reference

#16



reference

24

H&N dose accumulation





Dose difference relative Volume Histogram Parotids Right (blue) - left (green) If D>0 previsional dose > accumulated dose



Conclusions

- Adaptive RT: very useful, almost crucial, in a precise radiotherapy process
- On-line and off-line ART using cone-beam CT is much more common and can be easily used in all RT centres
- Even if it is true that in patients treated with RT, the doses required for ART procedures are very low, it is also true that the ALARA principle has to be adopted for each patient and optimization procedures should be much more diffused than now

Conclusion 2. Attention for the future

- Procedures of deformable image registration and dose accumulation are the key passages to obtain best dosimetric results by ART;
- ART with MRI will consent better target and OAR identification, non-invasive knowledge of tumour biology and can be used better personalize the treatment and the delivered dose
- Prospective studies integrating all these aspect are necessary to confirm the still embryonal data

Thank you for your attention

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