



Herbert Wertheim
College of Engineering
UNIVERSITY of FLORIDA

Modern Computational Phantoms and Their Applications

*Joint ICRP-RERF-JHPS Workshop
Recent Progress on Radiation Dosimetry for Epidemiology
and Radiological Protection
Sunday, December 2, 2017*

Wesley Bolch, University of Florida
ICRP Committee 2

POWERING THE NEW ENGINEER TO TRANSFORM THE FUTURE

Presentation Objectives

- 1. Review of different phantom format types – stylized, voxel, and hybrid*
- 2. Current series of phantoms used and adopted by ICRP – adult, pediatric, and pregnant female*
- 3. Review of different phantom morphometric categories – phantom libraries & individual-specific*
- 4. Example application of phantom libraries – pediatric CT radiation epidemiology*
- 5. Future phantoms from the ICRP – polygon mesh formats & tools for voxel-to-mesh conversion*

Computational Anatomic Phantoms

Essential tool for organ dose assessment

- **Definition** - *Computerized representation of human anatomy for use in radiation transport simulation of the medical imaging or radiation therapy procedure*

- **Need for phantoms vary across areas of radiological protection**
 - **Establishing dose coefficients for internal radiation exposure**
 - *Specific absorbed fractions for both self-dose and cross-dose to internal organs are computed using computational phantoms. These SAF values are then used, along with biokinetic models and radionuclide decay schemes, to compute dose coefficients - organ equivalent dose or effective dose per activity ingested or inhaled*
 - **Establishing dose coefficients for external radiation exposure**
 - *Either occupational or environmental fields of radiation or radionuclide emissions*
 - **Computing organ doses in radiological accidents – retrospectively / prospectively**

Computational Anatomic Phantoms

Essential tool for organ dose assessment

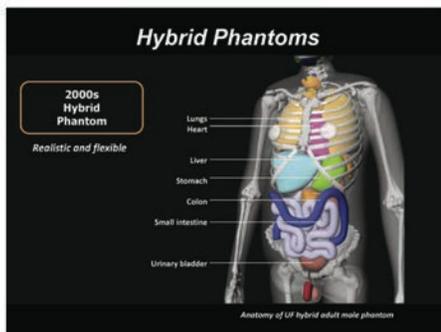
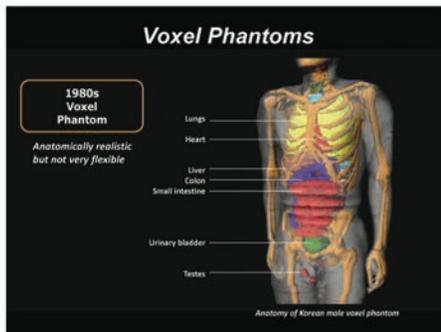
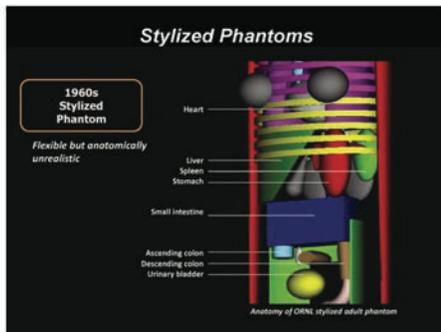
- **Definition** - *Computerized representation of human anatomy for use in radiation transport simulation of the medical imaging or radiation therapy procedure*

- **Need for phantoms vary with the medical application**
 - **Nuclear Medicine**
 - *3D patient images generally not available, especially for children*
 - **Diagnostic radiology and interventional fluoroscopy**
 - *No 3D image*
 - **Computed tomography**
 - *3D patient images available, problem – organ segmentation*
 - *No anatomic information at edges of scan coverage*
 - **Radiotherapy**
 - *Needed for characterizing out-of-field organ doses*
 - *Examples – IMRT scatter, proton therapy neutron dose*

Computational Anatomic Phantoms

Phantom Types and Morphometric Categories

- ***Phantom Format Types***
 - ⇒ *Stylized (or mathematical) phantoms*
 - ⇒ *Voxel (or tomographic) phantoms*
 - ⇒ *Hybrid (or NURBS/PM) phantoms*



Stylized (mathematical) phantoms
Flexible but anatomically unrealistic

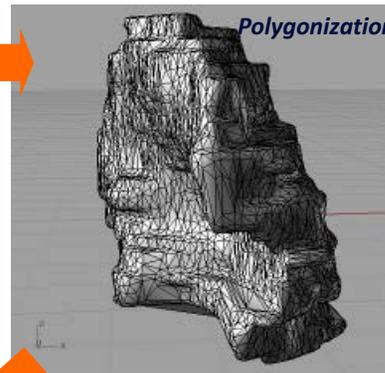
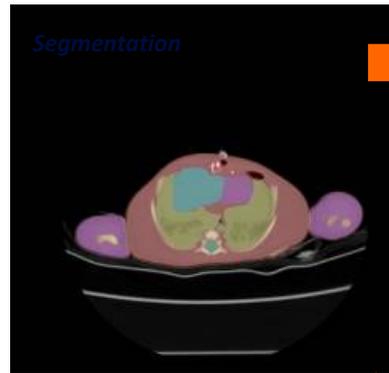
Voxel (tomographic) phantoms
Anatomically realistic but not very flexible

Hybrid (NURBS/Polygon Mesh) phantoms
Both anatomically realistic and flexible

Hybrid Phantom Construction

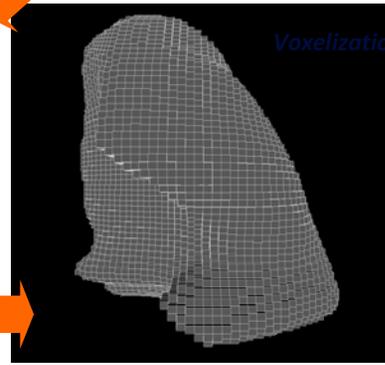
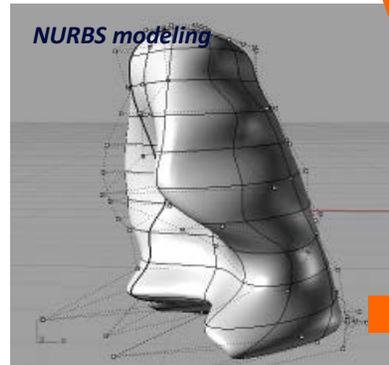
Example of the process used at the University of Florida

Segment patient CT images using 3D-DOCTOR™



Convert into polygon mesh using 3D-DOCTOR™

Make NURBS model from polygon mesh using Rhinoceros™



Convert NURBS model into voxel model using MATLAB code Voxelizer

Voxelizer Algorithm - See Phys Med Biol 52 (12) 3309-3333 (2007)

Computational Anatomic Phantoms

Phantom Types and Categories

■ Phantom Format Types

- ⇒ *Stylized (or mathematical) phantoms*
- ⇒ *Voxel (or tomographic) phantoms*
- ⇒ *Hybrid (or NURBS/PM) phantoms*

■ Phantom Morphometric Categories

- ⇒ *Reference (50th percentile individual, patient matching by age only)*
- ⇒ *Patient-dependent (patient matched by nearest height / weight)*
- ⇒ *Patient-sculpted (patient matched to height, weight, and body contour)*
- ⇒ *Patient-specific (phantom uniquely matching patient morphometry)*

Morphometric Categories – Reference Phantoms

Reference Individual - An idealised male or female with characteristics defined by the ICRP for the purpose of radiological protection, and with the anatomical and physiological characteristics defined in ICRP Publication 89 (ICRP 2002).

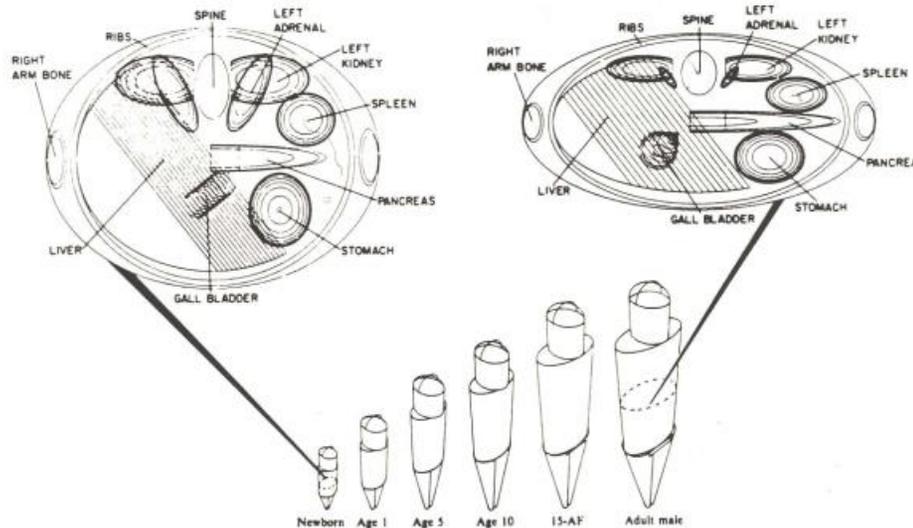
Table 2.9. Reference values for height, mass, and surface area of the total body

| Age | Height (cm) | | Mass (kg) | |
|----------|-------------|--------|-----------|--------|
| | Male | Female | Male | Female |
| Newborn | 51 | 51 | 3.5 | 3.5 |
| 1 year | 76 | 76 | 10 | 10 |
| 5 years | 109 | 109 | 19 | 19 |
| 10 years | 138 | 138 | 32 | 32 |
| 15 years | 167 | 161 | 56 | 53 |
| Adult | 176 | 163 | 73 | 60 |

Note – *While organ size / mass are specified in an ICRP reference phantom, organ shape, depth, position within the body are not defined by reference values*

Reference Phantoms Used by the ICRP

Until very recently, all dose coefficients published by the ICRP were based on computational data generated using the ORNL stylized phantom series.



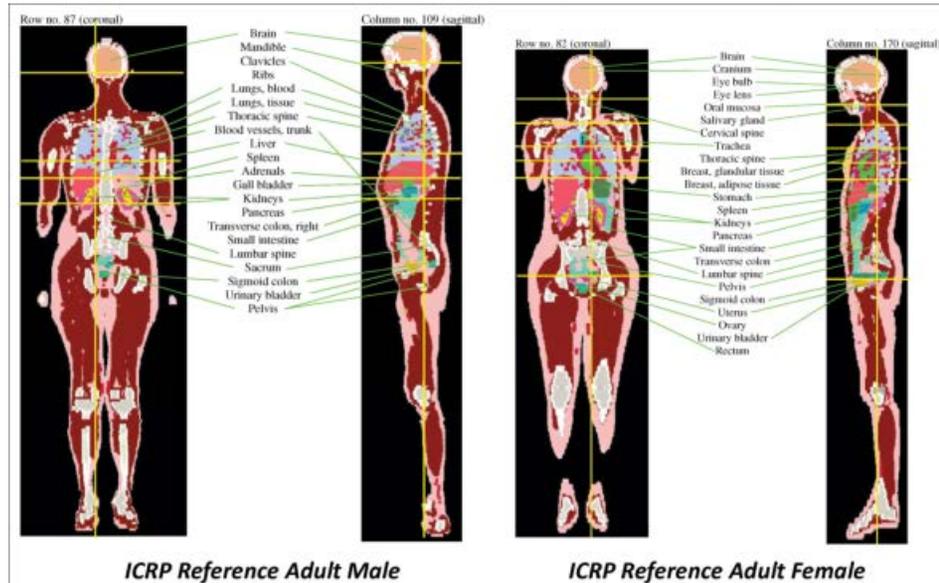
*ORNL TM-8381
Cristy & Eckerman*

Publications from ICRP using the Publication 110 Phantoms

- *ICRP Publication 116 – External Dose Coefficients (2010)*
- *ICRU Report 84 – Cosmic Radiation Exposure to Aircrew (2010)*
- *ICRP Publication 123 – Assessment of Radiation Exposure of Astronauts in Space (2013)*

Reference Phantoms Adopted by the ICRP

ICRP Publication 110 – Adult Reference Computational Phantoms

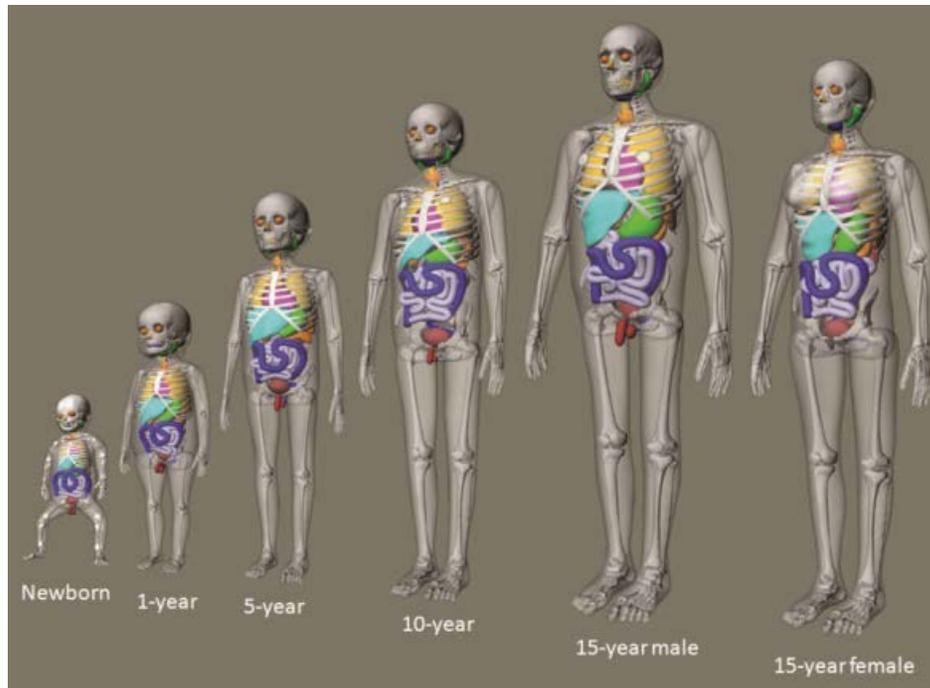


Publications from ICRP using the Publication 110 Phantoms

- **Publication 133 - Reference specific absorbed fractions (SAF) for internal dosimetry**
- **Publication 130 Series - Dose coefficients for radionuclide internal dosimetry following inhalation / ingestion**

Reference Phantoms Adopted by the ICRP

ICRPs upcoming reference phantoms for pediatric individuals are based upon the UF/NCI series of hybrid phantoms



IOP PUBLISHING

Phys. Med. Biol. 55 (2010) 339–363

Current Publications Under Development in ICRP Committee 2 Using Pediatric Phantoms

Task Group 90

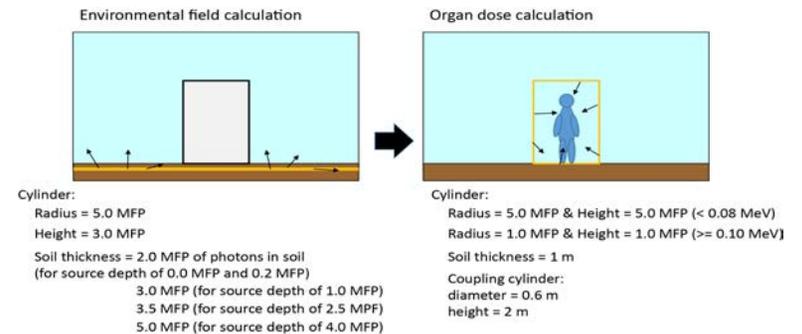
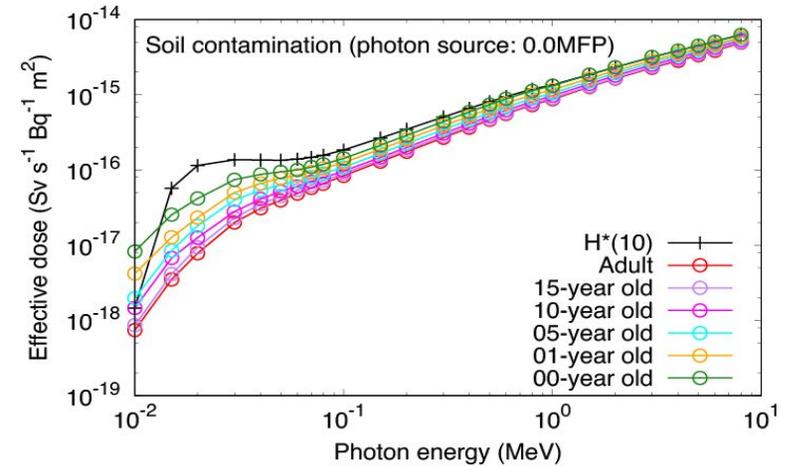
Dose Coefficients for Environmental External Exposures

Task Group 95

Dose Coefficients for Environmental Internal Exposures

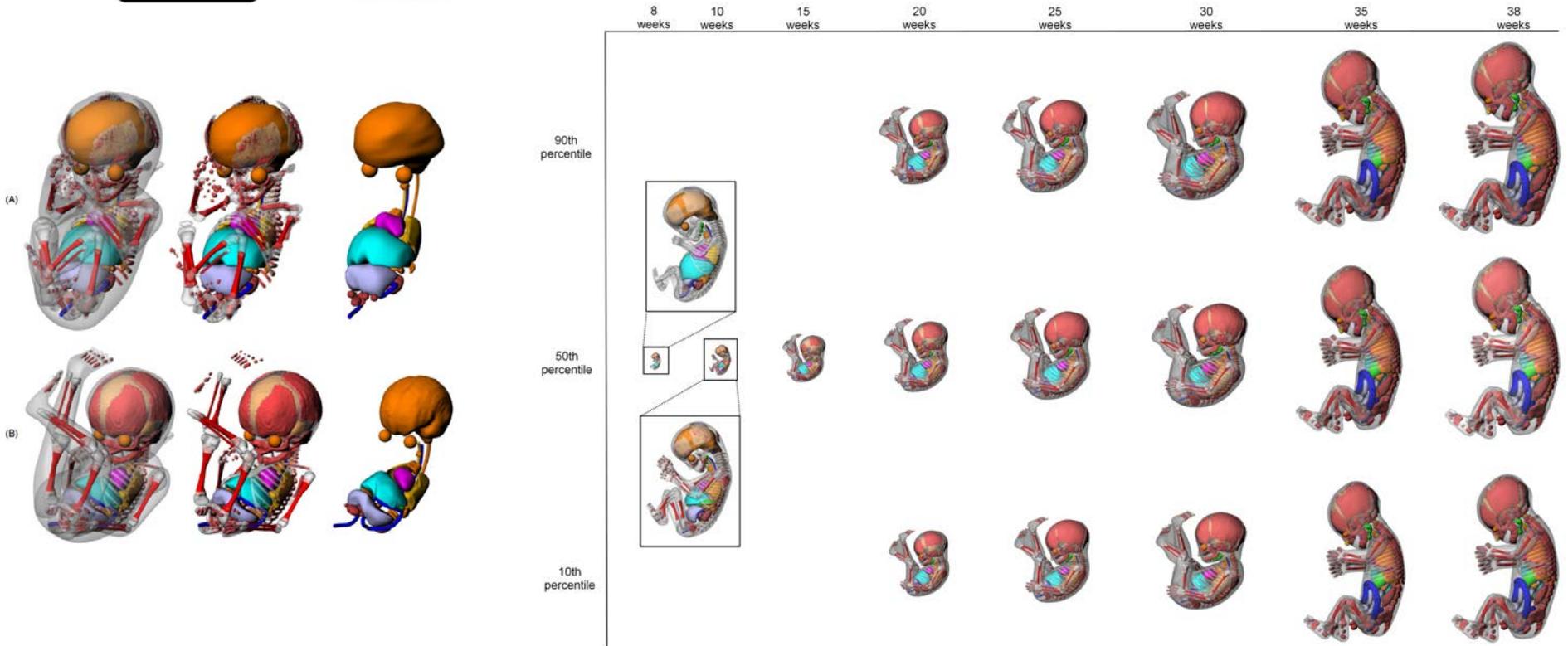
Task Group 96

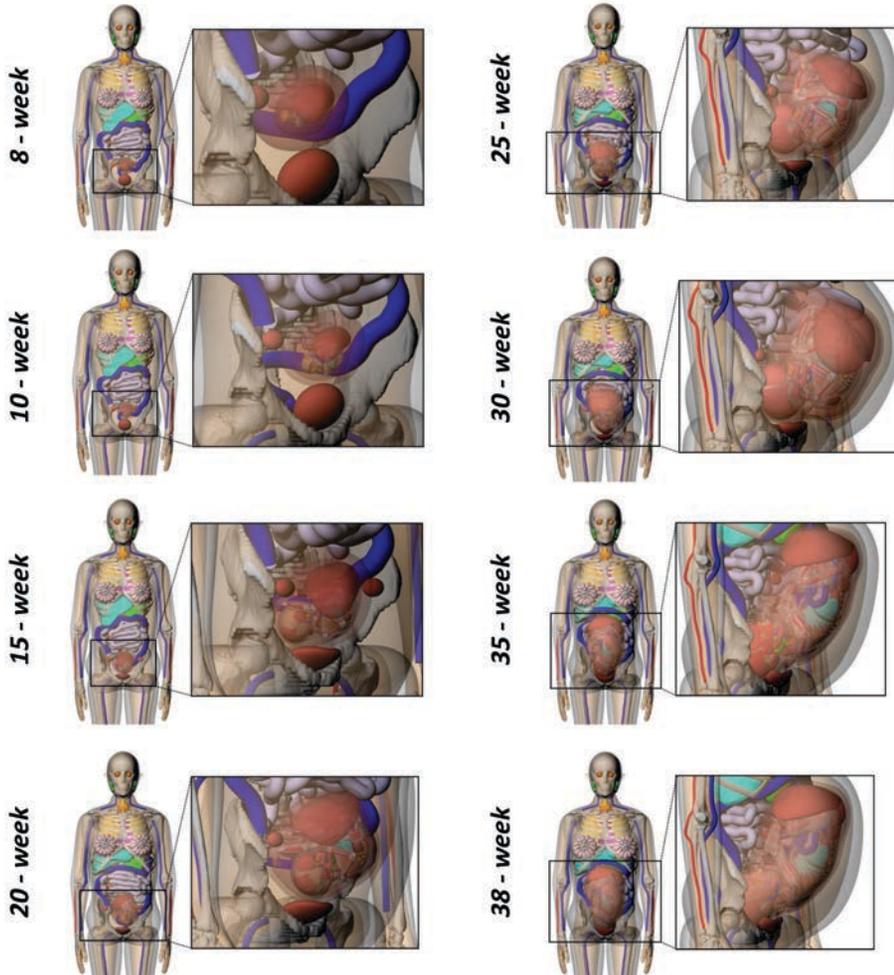
Specific Absorbed Fractions for Internal Exposures



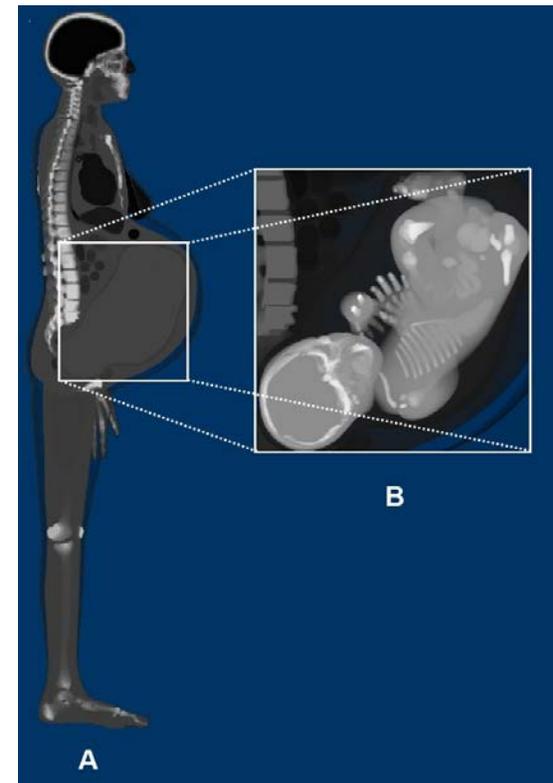


ICRP Series of Reference Fetal Models





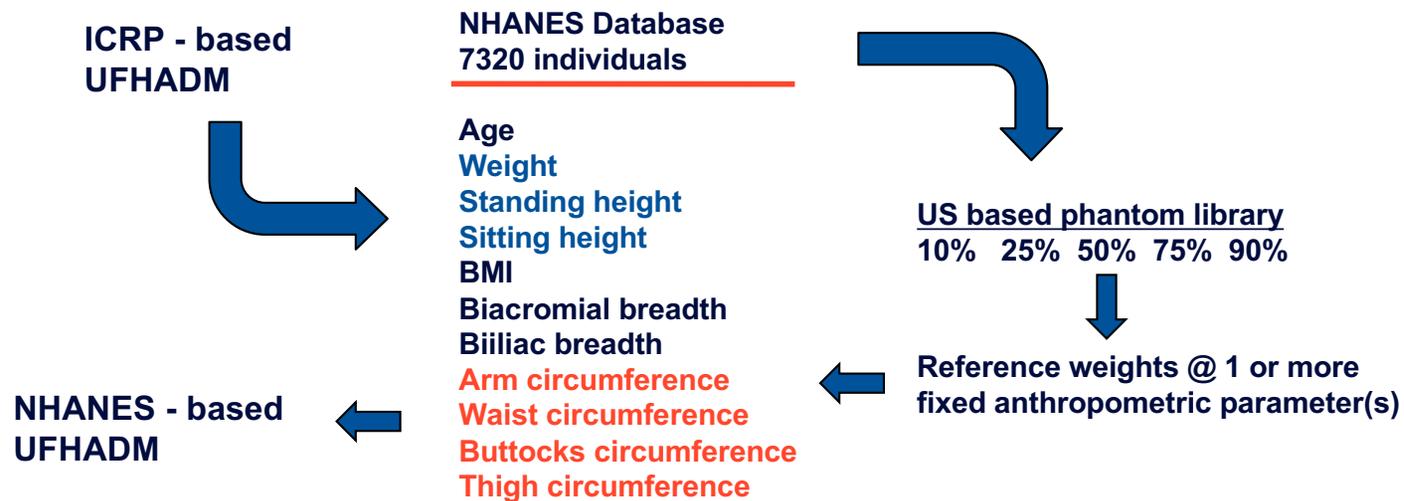
ICRP Series of Reference Pregnant Female Models



Morphometric Categories – Patient Dependent Phantoms

Definition -

Expanded library of reference phantoms covering a range of height / weight percentiles



Morphometric Categories – Patient Dependent Phantoms

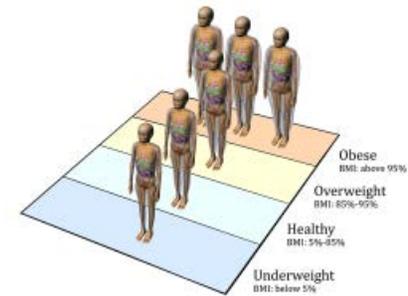
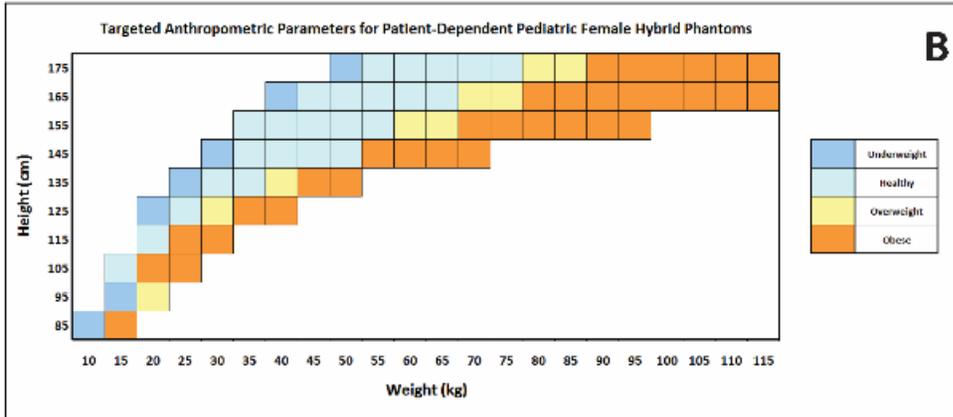
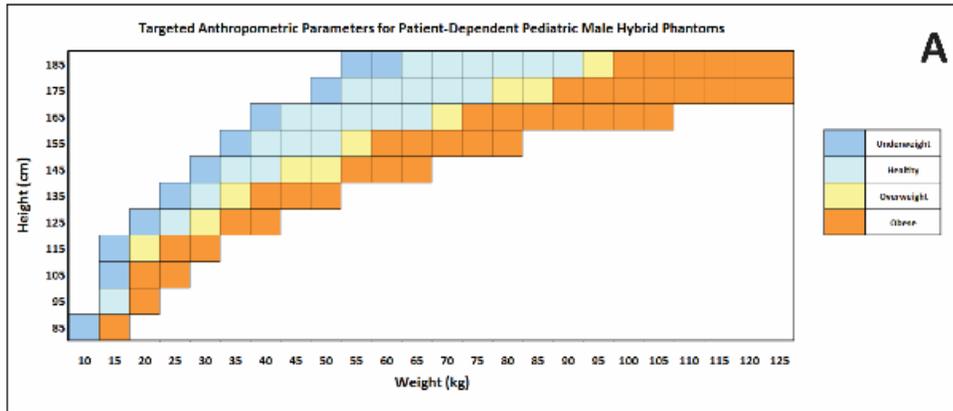
Patient-Dependent Hybrid Phantoms – UF Series

| Phantom Height (cm) | Pediatric | | Phantom Height (cm) | Adult | |
|------------------------|-----------|----------|------------------------|----------|----------|
| | Males | Females | | Males | Females |
| 185 | UFHADM ↑ | | 190 | UFHADM ↑ | |
| 175 | UFHADM ↓ | UFHADF ↑ | 185 | UFHADM ↑ | |
| 165 | UFH15M ↓ | UFHADF ↑ | 180 | UFHADM ↑ | |
| 155 | UFH15M ↓ | UFH15F ↓ | 175 | UFHADM ↓ | UFHADF ↑ |
| 145 | UFH10M ↑ | UFH10F ↑ | 170 | UFH15M ↑ | UFHADF ↑ |
| 135 | UFH10M ↓ | UFH10F ↓ | 165 | UFH15M ↓ | UFHADF ↑ |
| 125 | UFH10M ↓ | UFH10F ↓ | 160 | UFH15M ↓ | UFH15F ↓ |
| 115 | UFH05M ↑ | UFH05F ↑ | 155 | | UFH15F ↓ |
| 105 | UFH05M ↓ | UFH05F ↓ | 150 | | UFH15F ↓ |
| 95 | UFH05M ↓ | UFH05F ↓ | | | |
| 85 | UFH01M ↑ | UFH01F ↑ | | | |

The naming convention for the UF phantom series begins with the identifier UFH (University of Florida Hybrid), followed by the reference phantom age in years (00, 01, 05, 10, 15 and AD for adult) and then the phantom gender (M for male and F for female).

Geyer et al. – Phys Med Biol (2014)

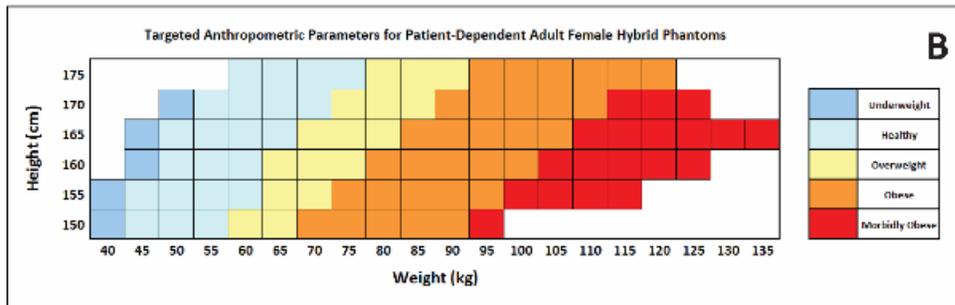
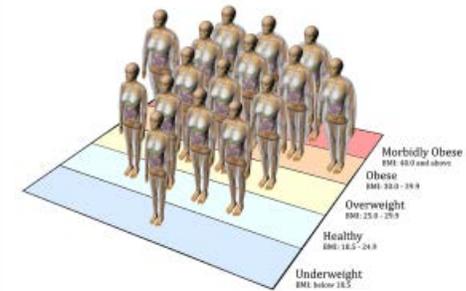
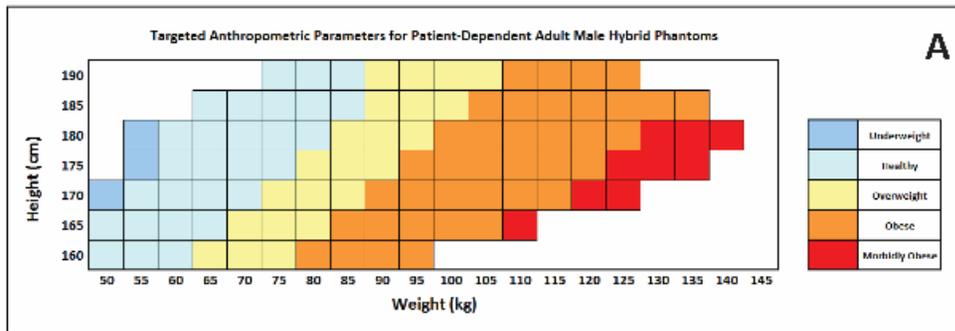
UF/NCI Phantom Library - Children



Phantom for each height/weight combination further matching average values of body circumference from CDC survey data

*85 pediatric males
73 pediatric females*

UF/NCI Phantom Library - Adults



Phantom for each height/weight combination further matching average values of body circumference from CDC survey data

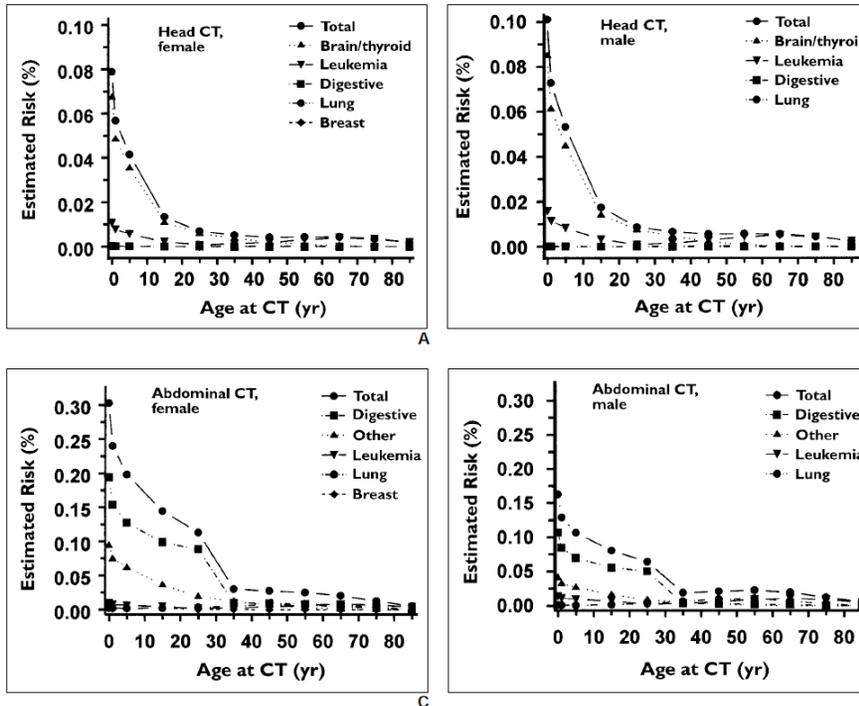
100 adult males
93 adult females

Article from Brenner et al. 2001 which changed CT imaging practice worldwide

Estimated Risks of Radiation-Induced Fatal Cancer from Pediatric CT

David J. Brenner¹
 Carl D. Elliston¹
 Eric J. Hall¹
 Walter E. Berdon²

AJR 2001;176:289–296



RESULTS. The larger doses and increased lifetime radiation risks in children produce a sharp increase, relative to adults, in estimated risk from CT. Estimated lifetime cancer mortality risks attributable to the radiation exposure from a CT in a 1-year-old are 0.18% (abdominal) and 0.07% (head)—an order of magnitude higher than for adults—although those figures still represent a small increase in cancer mortality over the natural background rate. In the United States, of approximately 600,000 abdominal and head CT examinations annually performed in children under the age of 15 years, a rough estimate is that 500 of these individuals might ultimately die from cancer attributable to the CT radiation.

Simplistic methods of organ dose

An Approach for the Estimation of Effective Radiation Dose at CT in Pediatric Patients¹

Radiology 1997; 203:417–422



Responses to Brenner Article:

- ***Development of professional society alliances – Image Gently, Step Lightly, Go with the Guidelines***
- ***Development of size-specific and standardized imaging protocols***
- ***Development of new technologies***
 - ***Tube current modulation in CT***
 - ***Improved detector techniques***
 - ***Improved image reconstruction algorithms***

Distinction between...

Risk projection – organ dose estimates coupled with existing cancer risk models

Risk assessment – direct measure of cancer risk through epidemiology studies

Radiation exposure from CT scans in childhood and subsequent risk of leukaemia and brain tumours: a retrospective cohort study

Mark S Pearce, Jane A Salotti, Mark P Little, Kieran McHugh, Choonsik Lee, Kwang Pyo Kim, Nicola I Howe, Cecile M Ronckers, Preetha Rajaraman, Sir Alan W Craft, Louise Parker, Amy Berrington de González

www.thelancet.com Vol 380 August 4, 2012

Use of CT scans in children to deliver cumulative doses of about 50 mGy might almost triple the risk of leukaemia and doses of about 60 mGy might triple the risk of brain cancer. Because these cancers are relatively rare, the cumulative absolute risks are small: in the 10 years after the first scan for patients younger than 10 years, one excess case of leukaemia and one excess case of brain tumour per 10 000 head CT scans is estimated to occur. Nevertheless, although clinical benefits should outweigh the small absolute risks, radiation doses from CT scans ought to be kept as low as possible and alternative procedures, which do not involve ionising radiation, should be considered if appropriate.

Cancer risk in 680 000 people exposed to computed tomography scans in childhood or adolescence: data linkage study of 11 million Australians

John D Mathews *epidemiologist*¹, Anna V Forsythe *research officer*¹, Zoe Brady *medical physicist*², Martin W Butler *data analyst*³, Stacy K Goergen *radiologist*⁴, Graham B Byrnes *statistician*⁵, Graham G Giles *epidemiologist*⁶, Anthony B Wallace *medical physicist*⁷, Philip R Anderson *epidemiologist*^{8,9}, Tenniel A Guiver *data analyst*³, Paul McGale *statistician*¹⁰, Timothy M Cain *radiologist*¹¹, James G Dowty *research fellow*¹, Adrian C Bickerstaffe *computer scientist*¹, Sarah C Darby *statistician*¹⁰

BMJ 2013;346:f2360

The increased incidence of cancer after CT scan exposure in this cohort was mostly due to irradiation. Because the cancer excess was still continuing at the end of follow-up, the eventual lifetime risk from CT scans cannot yet be determined. Radiation doses from contemporary CT scans are likely to be lower than those in 1985-2005, but some increase in cancer risk is still likely from current scans. Future CT scans should be limited to situations where there is a definite clinical indication, with every scan optimised to provide a diagnostic CT image at the lowest possible radiation dose.

Risk of Pediatric and Adolescent Cancer Associated with Medical Imaging

R01 CA185687

The use of medical imaging that delivers ionizing radiation is high in the United States. The potential harmful effects of this imaging must be understood so they can be weighed against its diagnostic benefits, and this is especially critical for our vulnerable populations of children and pregnant women. The proposed study will comprehensively evaluate patterns of medical imaging, cumulative exposure to radiation, and subsequent risk of pediatric cancers in four integrated health care delivery systems comprising over 7 million enrolled patients enrolled from 1996-2017.

Project Management

University of California, San Francisco (UCSF)

Biostatistics and Epidemiology

University of California, Davis (UCD)

Organ Dose Assessment

University of Florida (UF)

Patient Enrollment Sites

Kaiser Permanente Northern California (KPNC)

Kaiser Permanente North West (KPNW)

Kaiser Permanente Hawaii (KPHI)

Kaiser Permanente Washington (KPWA)

Marshfield Clinic Research Institute (MCRI)

Pediatric Oncology Group of Ontario (POGO)

Geisinger Health Systems (GE)

Harvard Pilgrim Health Plan (HP)

***Risk of Pediatric and Adolescent Cancer Associated with Medical Imaging
R01 CA185687***

Aim 1: Imaging Utilization Patterns

Aim 1A – Patterns of imaging utilization in pregnant women

Aim 1B – Patterns of imaging utilization in children

Aim 1C – Patterns of imaging utilization in adults and children

Aim 2: Organ Dose and Association with Cancer Outcomes

Aim 2A – Imaging in pregnant women and childhood cancer risk

Aim 2B – Imaging in children and childhood leukemia risk

Aim 2C – Imaging in pregnant women and children and childhood cancer risk

1. Organ Dose Reconstruction in Computed Tomography

Data Collection – 2006 to 2017

Data Collection – 1996 to 2006

Radimetrics

Data Abstraction

Patient Data

Study ID

Age

Gender

Height

Weight

Effective diameter at center slice (cm)

Pregnant Females

Gestational age

CT Procedure Details

Year of scan

Scan # in current year

Series # in current scan

Body part imaged

Medical facility

CT scanner manufacturer

CT scanner model

CT Technique Factors

Scan length (cm)

Beam collimation (mm)

Beam energy (kVp)

Pitch

CTDIvol (mGy)

DLP (mGy-cm)

Fixed or modulated mA

Exam Averaged mAs

CT computational methodology – Fixed Tube Current

$$NF_{E,C} \left(\frac{\text{photons}}{\text{mAs}} \right) = \frac{\text{Air Kerma}_{\text{measured}} \left(\frac{\text{mGy}}{\text{mAs}} \right)}{\text{Air Kerma}_{\text{simulated}} \left(\frac{\text{mGy}}{\text{photon}} \right)}$$

$$\text{Organ Dose} \left(\frac{\text{mGy}}{\text{mAs}} \right) = \left[\sum_{i=Z_{\text{exam start}}}^{Z_{\text{exam end}}} \text{Organ Dose}_i \left(\frac{\text{mGy}}{\text{photon}} \right) \right] \times NF_{E,C} \left(\frac{\text{photons}}{\text{mAs}} \right)$$

Physical validation of a Monte Carlo-based, phantom-derived approach to computed tomography organ dosimetry under tube current modulation

Elliott J. Stepusin
J Crayton Pruitt Family Department of Biomedical Engineering, University of Florida, Gainesville, FL 32611-6131, USA
Daniel J. Long
Department of Medical Physics, Memorial Sloan Kettering Cancer Center, 1275 York Avenue, New York, NY 10065, USA
Kayla R. Ficarrotta,* David E. Hintenlang,¹ and Wesley E. Bolch^{¶1}
J Crayton Pruitt Family Department of Biomedical Engineering, University of Florida, Gainesville, FL 32611-6131, USA

Med. Phys. 44 (10), October 2017

CT computational methodology – Modulated Tube Current

$$\text{Effective mAs} = \frac{(\text{Exam Average mA}) \times \text{Rotation Time (s)}}{\text{Exam Pitch}}$$

$$WF(z) = \frac{AV_{\text{average}}(z)}{\sum_{i=Z_{\text{exam start}}}^{Z_{\text{exam end}}} AV_{\text{average},i}}$$

$$\text{Organ Dose (mGy)} = \left[\sum_{i=Z_{\text{exam start}}}^{Z_{\text{exam end}}} \text{Organ Dose}_i \left(\frac{\text{mGy}}{\text{mAs}} \right) \times WF_i \right] \times \text{Effective mAs}$$

Six Methods of Patient-to-Phantom Matching for CT Organ Dosimetry

1. **Patient Age/Gender Only**
2. **Height and Weight**

UF/NCI Reference Phantom
UF/NCI Library Phantom

3. **Effective Diameter – Scan Averaged**
4. **Effective Diameter – Center Slice**

UF/NCI Library Phantom
UF/NCI Library Phantom

$$\text{Effective Diameter (cm)} = \sqrt{\text{Diameter}_{\text{Lateral}}(\text{cm}) \times \text{Diameter}_{\text{AP}}(\text{cm})}$$

AAPM Task Group 204

5. **Water Equivalent Diameter – Scan Averaged**
6. **Water Equivalent Diameter – Center Slice**

UF/NCI Library Phantom
UF/NCI Library Phantom

$$\text{Water Equivalent Diameter (cm)} = 2 \sqrt{\left[\frac{1}{1000} \overline{CT(x,y)_{ROI}} + 1 \right] \frac{A_{ROI}(\text{cm}^2)}{\pi}}$$

AAPM Task Group 220

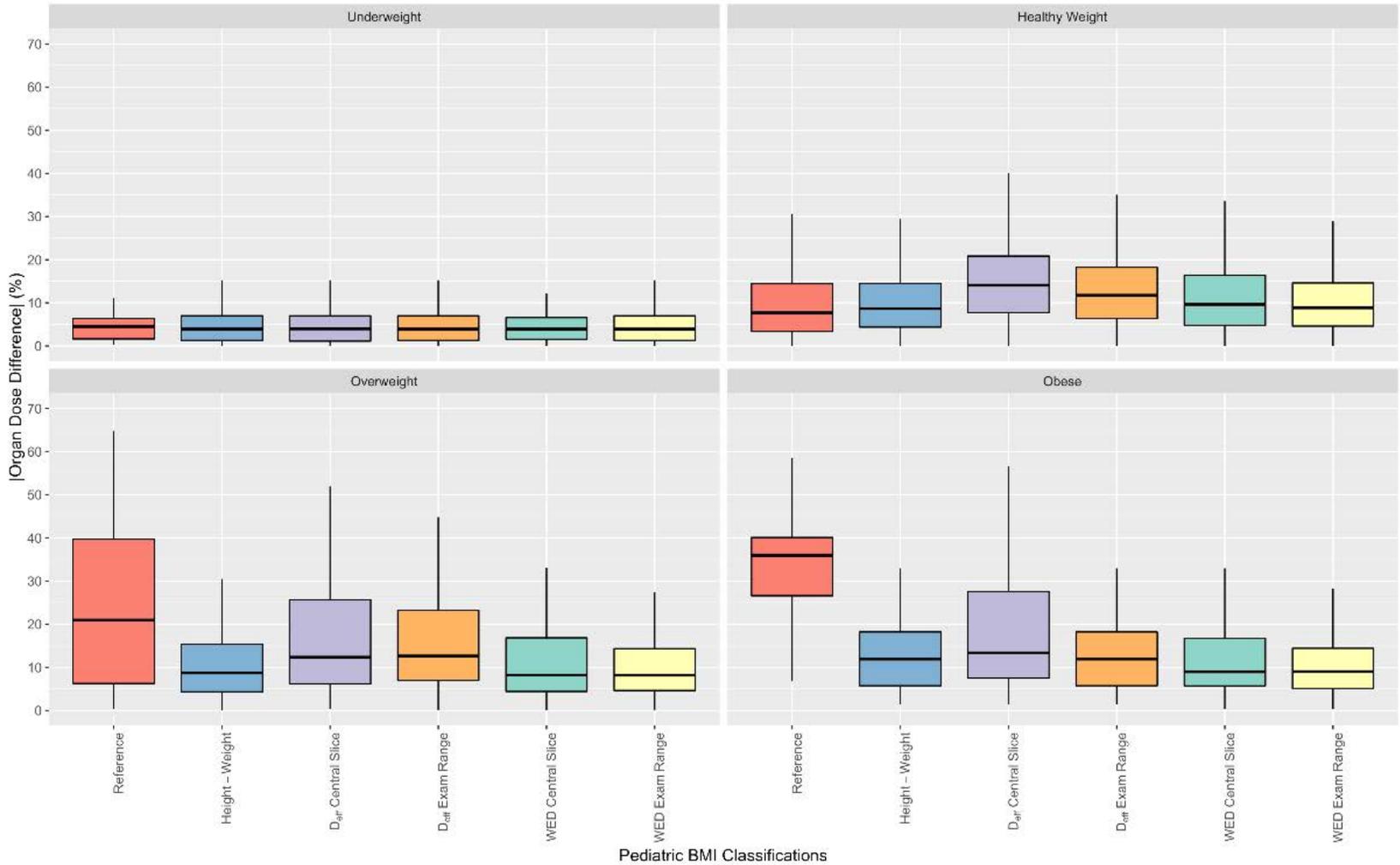
$$CT(x,y) = \left(\frac{\mu(x,y) - \mu_{\text{water}}}{\mu_{\text{water}}} \right) \times 1000 \quad \tilde{\mu} = \rho \times \sum_i^{N_c} \left[\sum_j^{N_e} \left(w_i \left(\frac{\mu}{\rho} \right)_{i,j} p_j \right) \right]$$

Assessment of different patient-to-phantom matching criteria applied in Monte Carlo-based computed tomography dosimetry

Elliott J. Stepusin
J. Crayton Pruitt Family Department of Biomedical Engineering, University of Florida, Gainesville, FL 32611-6131, USA
Daniel J. Long
Department of Medical Physics, Memorial Sloan Kettering Cancer Center, 1275 York Avenue, New York, NY 10065, USA
Emily L. Marshall and Wesley E. Bolch^{*)}
J. Crayton Pruitt Family Department of Biomedical Engineering, University of Florida, Gainesville, FL 32611-6131, USA

Med. Phys. 44 (10), October 2017

Boxplots comparing organ dose percent difference for each of the six matching parameters based on CDC BMI classifications for pediatric patients. The vertical lines extend at most 1.5 times the interquartile range.



2. Organ Dose Reconstruction in Diagnostic Fluoroscopy

Data Collection – 2006 to 2017

Data Collection – 1996 to 2006

Radimetrics

Data Abstraction

Patient Data

Study ID
Age
Gender
Height
Weight

Fluoroscopy Procedure Details

Procedure type (1 to 6)
Cumulative fluoroscopy time
Cumulative reference air kerma
Cumulative kerma-area product

Reference Fluoroscopy Exams

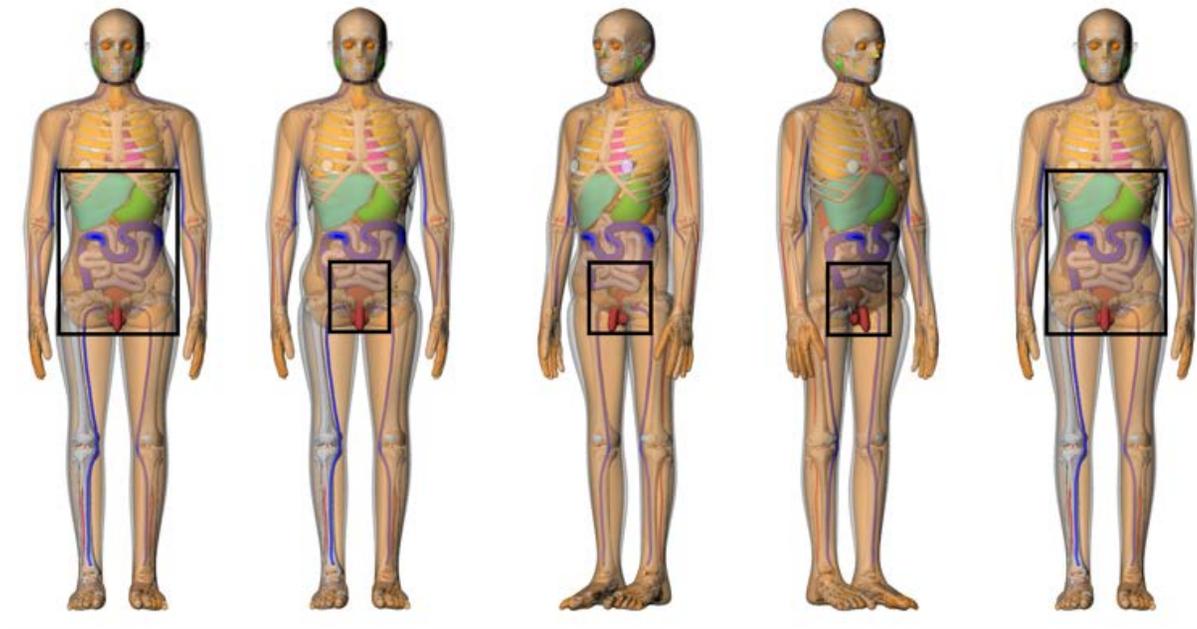
1. Upper Gastrointestinal Series (UGI)
2. Upper Gastrointestinal Series with Follow-Through (UGI-FT)
3. Voiding Cystourethrogram (VCUG)
4. Rehabilitation Swallow (RS)
5. Lower Gastrointestinal Series / Barium Enema (LGI)
6. Gastrostomy Tube Placement (G-Tube)

Problem – nearly all diagnostic fluoroscopy systems cannot generate RDSRs

Solution – create “reference” diagnostic exams and scale doses by FT, RAK, KAP

Diagnostic Fluoroscopy Procedure Outlines - UF

VCUG Procedure Duration: 120 seconds



| | | | | |
|----------------|-------------------------------------|-------------------------------------|-------------------------------------|--------------------------------------|
| Image 1: 5% | Image 2: 9% | Image 3: 8% | Image 4: 8% | Image 5: 16% |
| Time: 6 s | Time: 10.8 s | Time: 9.6 s | Time: 9.6 s | Time: 19.2 s |
| Contrast: None | Contrast: 50% concentration bladder | Contrast: 50% concentration bladder | Contrast: 50% concentration bladder | Contrast: 100% concentration bladder |

Iodine Contrast 

3. Organ Dose Reconstruction in Diagnostic Nuclear Medicine

Data Collection – 2006 to 2017

Data Collection – 1996 to 2006

Radimetrics

Data Abstraction

Patient Data

Study ID
Age
Gender
Height
Weight

NM Procedure Details

Procedure type (1 to 6)
Administered Activity

Reference NM Procedures

1. Tc-99m DMSA
2. Tc-99m MDP
3. Tc-99m MAG3
4. F-18 FDG
5. Tc-99m Sulfur Colloid
6. I-123 MIBG

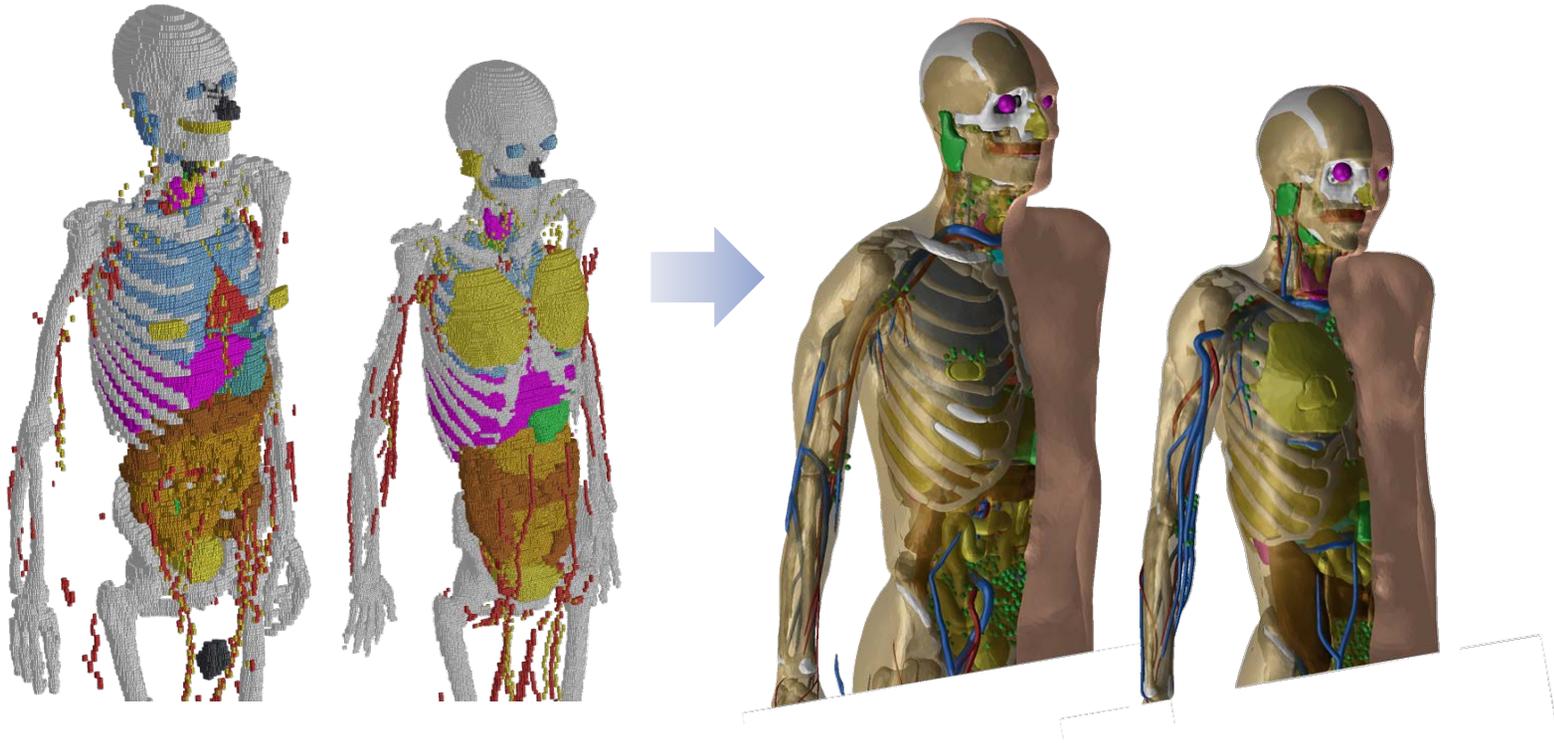
Problem – Injected activity might not be available

Solution – Use current guidelines or period-specific weight-based dosing schemes

Biokinetics – Assume ICRP reference models

Radionuclide S values – Assume values from the UF reference phantoms

Committee 2 Task Group 103



VRCPs
(Voxel-type Reference Computational Phantoms)
(ICRP Publication 110)

MRCPs
(Mesh-type Reference Computational Phantoms)

Figure courtesy of CH Kim – TG 103 Chair

Computation Speed - PHITS

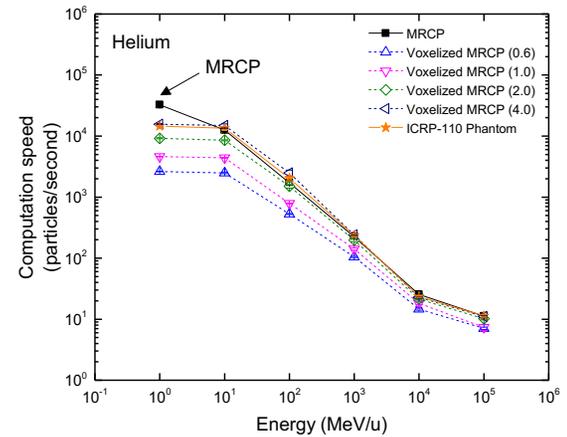
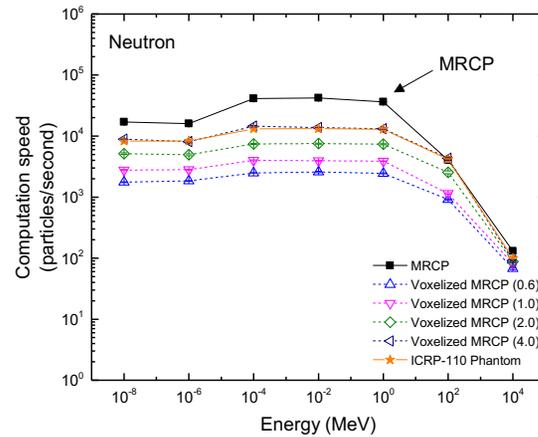
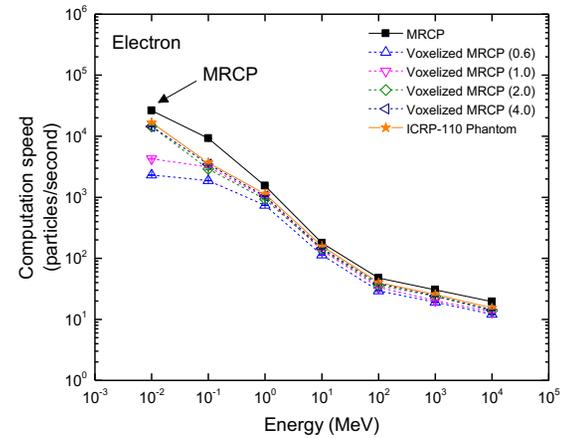
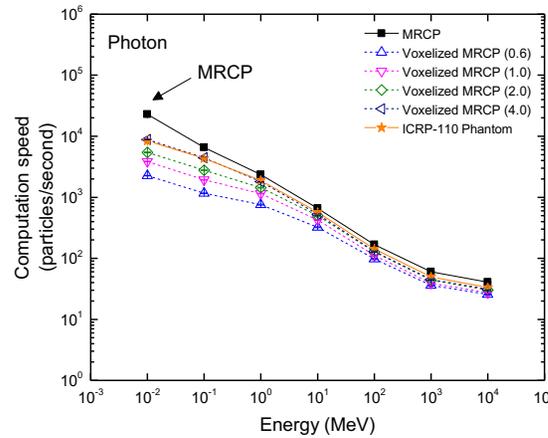
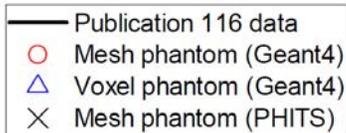
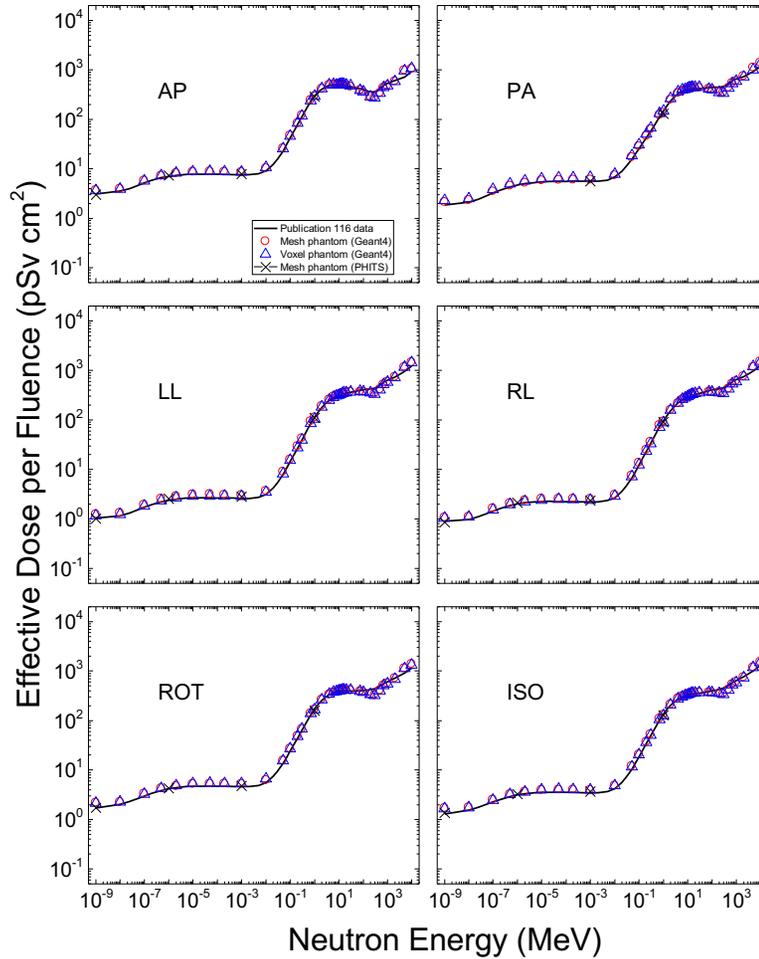


Figure courtesy of CH Kim – TG 103 Chair

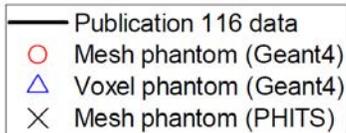
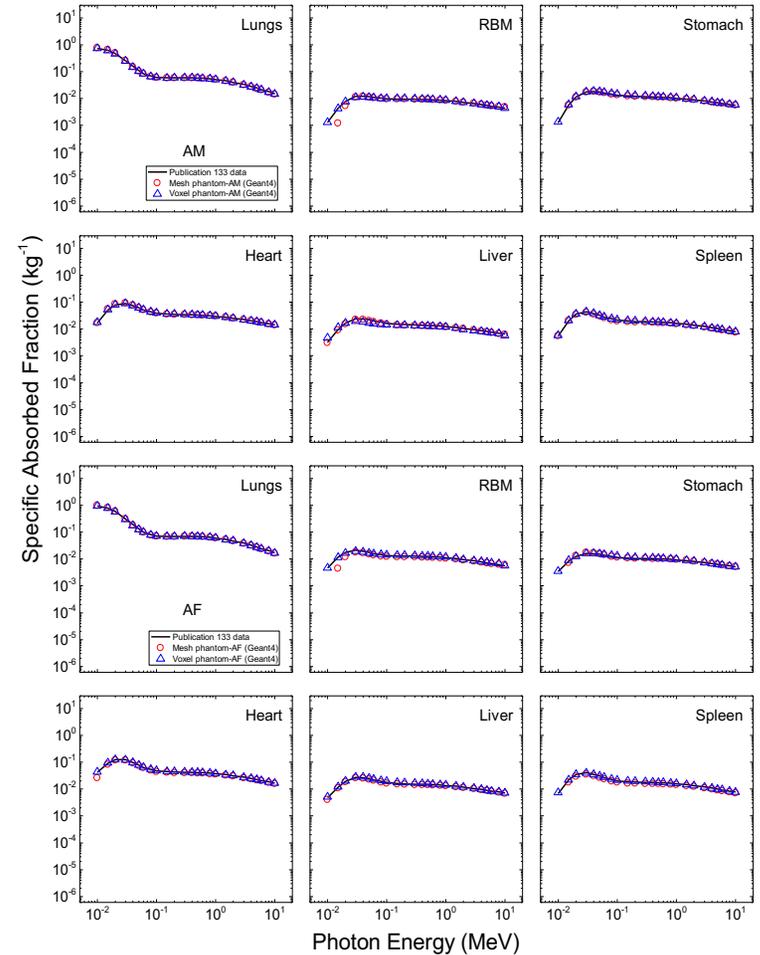
Important Conclusion –

Use of Mesh-Type Phantoms Dose Not Alter In Any Meaningful Way Dose Coefficients Previously Published by ICRP

Effective Dose - Neutron

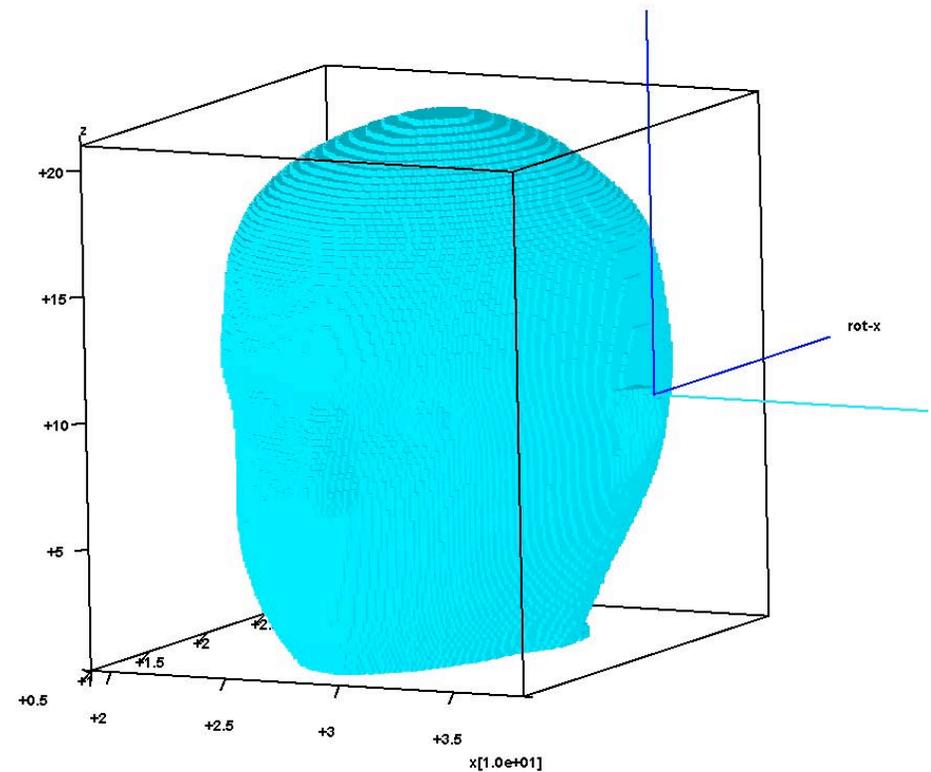


Source: Lungs



Recently Developed Voxel to TM Algorithm

- *Successful conversion of voxel phantom to surface meshed phantom with unique vertices*
- *Surface mesh ready for Tetgen™ to generate tetrahedral mesh*
- *Joint collaboration between UF and JAEA (manuscript in preparation)*





Thank you for your attention!



東京大学
THE UNIVERSITY OF TOKYO

